

### **Amendments to the Specification:**

Please amend paragraph [0013] to read as follows:

[0013] As illustrated in Fig. 1, a refocused SSFP sequence consists of a single RF excitation which is repeated periodically. All gradients used for slice selection or imaging are fully rewound over each repetitive time, TR. **In Points a, b, c, d are along the time axis, and** the steady-state, the magnetization at points a and d is the same.

Please amend paragraph [0016] to read as follows:

[0016] All imaging gradients are rewound, and the low spatial frequency-information is acquired at an echo time (TE) **less than TR, and in this embodiment** midway between RF excitation pulses. The steady-state signal that arises after many repetitions is shown in Fig. 2A. The signal magnitude is a strong function of the resonant frequency, with signal nulls spaced apart by  $1/TR$ . The magnitude also varies for different relaxation times  $T_1$  and  $T_2$  as is typical for MRI sequences.

Please amend paragraph [0024] to read as follows:

[0024] The invention applies to a standard SSFP imaging sequence where the echo time **is less than TR and can be** ~~[[is]]~~ midway between RF excitation pulses. The most common such method is simple Cartesian imaging. However, the method will also work for radial SSFP imaging, echo-planar SSFP imaging, or spiral in-out imaging.

Please amend paragraph [0027] to read as follows:

[0027] There has been described a new, rapid material suppressed imaging technique using standard SSFP imaging with a phase-sensitive reconstruction. The invention exploits the refocusing property of SSFP to provide a robust fat-suppression technique that is only as sensitive to off resonance as the SSFP sequence itself. In using standard SSFP imaging, the repetition time (TR) is approximately equal to the reciprocal of chemical shift between lipid and water, and the effective echo time (TE) is **less than TR and can be** equal to  $TR/2$ .